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Digital detection and processing of multiple quadrature harmonics for EPR spectroscopy

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ABSTRACT

A quadrature digital receiver and associated signal estimation procedure are reported for L-band electron paramagnetic resonance (EPR) spectroscopy. The approach provides simultaneous acquisition and joint processing of multiple harmonics in both in-phase and out-of-phase channels. The digital receiver, based on a high-speed dual-channel analog-to-digital converter, allows direct digital down-conversion with heterodyne processing using digital capture of the microwave reference signal. Thus, the receiver avoids noise and nonlinearity associated with analog mixers. Also, the architecture allows for low-Q anti-alias filtering and does not require the sampling frequency to be time-locked to the microwave reference. A noise model applicable for arbitrary contributions of oscillator phase noise is presented, and a corresponding maximum-likelihood estimator of unknown parameters is also reported. The signal processing a convergent iterative algorithm capable of jointly processing the in-phase and out-of-phase data in the presence of phase noise and unknown microwave phase. Cramér-Rao bound analysis and simulation results demonstrate a significant reduction in linewidth estimation error using quadrature detection, for both low and high values of phase noise. EPR spectroscopic data are also reported for illustration.

1. Introduction

Electron paramagnetic resonance (EPR) is a spectroscopic method capable of detecting free radicals. Over the past several decades, EPR has found numerous applications in biology, chemistry, physics, and medicine [1]. For biological applications, such as *in vivo* oximetry [2–4], there exists a pressing need to speed up the data acquisition process for EPR spectroscopy and imaging [5].

For EPR, the data are collected by measuring the absorption of electromagnetic radiation, usually in the microwave range, by paramagnetic species in the presence of an external magnetic field. For imaging applications, an additional magnetic field, in the form of a linear magnetic field gradient, is applied to provide spatial encoding. Recent efforts to accelerate EPR data collection include both hardware and algorithm developments. For example, overmodulation [6], fast scan [7], rapid scan [8], pulsed EPR [9,10], parametric modeling [11], adaptive and uniform data sampling [12,13], and multisite oximetry [14,15] have shown potential to accelerate the acquisition process.

The microwave signal reflected from the EPR sample cavity, also called resonator, experiences changes in both amplitude and phase

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upon magnetic resonance. These changes encode the absorption and dispersion components of the EPR spectra. To avoid 1/*f* noise, associated with both the microwave source and the diode detector commonly employed to demodulate the EPR signal to baseband, it is a common practice to apply field modulation. The process of EPR signal extraction then reduces to diode detection followed by phase sensitive detection (PSD) [16]. Inclusion of automatic frequency control (AFC), in its typical configuration [17], allows capturing an absorption harmonic. Other AFC configurations allow collection of a dispersion harmonic instead [18].

Homodyne detection, involving magnetic field modulation and PSD, remains the most prevalent configuration for CW EPR spectrometers. An obvious limitation of homodyne detection is the inability to collect multiple field modulation harmonics simultaneously. For cases where the field modulation amplitude approaches or exceeds the intrinsic linewidth of the paramagnetic specie, a significant fraction of energy resides in higher harmonics. Therefore, quadrature detection across multiple harmonics can reduce the data collection time, or, equivalently, can improve the signal-to-noise ratio (SNR).

Hyde et al. [19] were the first to demonstrate a technique, using digital heterodyne reception, to simultaneously collect absorption and dispersion spectra across multiple harmonics. Several prototypes were presented [20] to implement the digital receiver. The basic configuration included: (i) down-conversion





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of the microwave signal (reflected from the sample cavity) to an intermediate frequency (IF), (ii) time-locked subsampling of the IF signal without inducing aliasing, and (iii) digital matched filtering. In 2008, Yen [21] reported linewidth estimation error analysis for jointly processing multiple quadrature harmonics of a Lorentzian lineshape. More recently, Tseitlin et al. [22,23] reported implementation of a digital heterodyne receiver to collect multiple harmonics of absorption and used nonlinear curve fitting to estimate Lorentzian linewidth information.

In this work, we present a direct digital receiver design and briefly outline its implementation. The receiver utilizes a highspeed dual-channel analog-to-digital converter (ADC) to simultaneously sample the bandpass signals from both the microwave source and the circulator which carries the reflected signal from the sample cavity. Direct digital conversion avoids noise and nonlinear distortion associated with analog mixers. Further, this configuration does not require the sampling frequency to be time-locked to the microwave reference [19]. Unlike previously reported work [22], which processed the absorption data alone, we present a framework to jointly process multiple harmonics for quadrature channels. In addition, our proposed processing is capable of handling unequal noise powers between the quadrature channels, for instance due to phase noise of the microwave source. Other benefits of the proposed receiver and processing include modeling and recovery of nuisance parameters including microwave phase, baseline distortion, and magnetic field drift.

The remainder of the paper is organized as follows: Section 2 describes the instrumentation and the processing approach to jointly estimate unknown parameters including linewidth, spin density, microwave phase, baseline offset and slope, center field, and modulation amplitude; Section 3 presents results from simulation and an L-band spectroscopy experiment; Section 4 includes discussion; Section 5 summarizes the conclusions; and Appendix A provides derivation of an EPR noise model applicable to cases with nonnegligible phase noise contributions.

2. Methodology

Digital detection offers several advantages over the traditional homodyne detection, including collection of multiple harmonics and flexibility of retrospective signal processing. However, implementation of a digital receiver poses unique technical challenges. In this section, we briefly overview the proposed digital receiver design, highlighting its differences from existing designs. Also, we present a convergent iterative processing scheme for maximum-likelihood estimation of the unknown parameters under nonideal conditions, such as in the presence of phase noise, unknown microwave phase, and baseline drift.

2.1. Receiver overview

The basic operation of digital down-conversion via sub-Nyquist sampling of a bandpass signal is illustrated in Fig. 1. The microwave signal reflected from the resonator (Fig. 1i) is amplified and bandpass filtered before it is sampled in channel 1 of the ADC. The signal is bandpass in that it has bandwidth of approximately $2\pi \times 3 \times 10^6$ rad/s while the accompanying noise is bandpass with $2\pi \times 75 \times 10^6$ rad/s bandwidth defined by the bandpass filter. The signal, along with the noise, is centered on the carrier frequency, ω_c . By sampling at a rate, ω_s , below ω_c , aliases of the bandpass signal are replicated periodically, as depicted in Fig. 1iv. An appropriate selection of ω_s ensures that the replicas, called images, of the signal are disjoint in frequency, and hence that aliasing artifacts are avoided. For example, with $\omega_c = 2\pi \times 1.283 \times 10^9$ rad/s and $\omega_s = 2\pi \times 400 \times 10^6$ rad/s, an image of the original bandpass

microwave signal is centered at $2\pi \times 83 \times 10^6$ rad/s (i.e., $\omega_c - k\omega_s$ for k = 3); so, the $2\pi \times 75 \times 10^6$ rad/s bandwidth of the filtered microwave signal fits easily within the unaliased Nyquist zone, 0 to $\omega_s/2$. Thus, sampling effectively provides demodulation to a digital IF signal. (This is an example of sampling a bandpass signal in the seventh Nyquist zone [24].)

The microwave source signal is likewise bandpass filtered and is sampled in channel 2, thereby providing a reference for eventually digital demodulation from IF to baseband as shown in Fig. 1. Specifically, the contents of channel 1 (C_1) are digitally multiplied with the contents of channel 2 (C_2) and its Hilbert transform, (\check{C}_2) to generate in-phase (S_I) and out-of-phase (S_Q) baseband channels, respectively. While the two channels of the ADC are time-locked by virtue of a common sampling clock, the sampling clock is not time-locked to the microwave source in this architecture. Both (S_I) and (S_O) are then digitally cross-correlated with sinusoidal waveforms at the modulation frequency ω_m and its multiples to extract individual harmonics I1, I2, I3..., and Q1, Q2, Q3..., respectively. The sampled data streams, C_1 and C_2 , from each scan are decomposed into small blocks, and all the postprocessing is carried out on a block-by-block basis. The block size is chosen sufficiently small such that the swept magnetic field is approximately constant across a single block. In experiments reported here, 1024 blocks, each 38 ms in duration, were used to provide a total sweep width of 10 G in 3.9 s.

2.2. Hardware layout

Figs. 2 and 3 show the block diagram of the digital receiver and its interface with a CW EPR spectrometer, respectively. The microwave signal from the circulator is amplified using a 40 dB lownoise amplifier (LNA) and bandpass filtered using an analog filter with $2\pi \times 75 \times 10^6$ rad/s bandwidth before being fed to channel 1 of the ADC. The signal from the microwave source, a cavity oscillator in this case, is bandpass filtered using a similar analog filter before being fed to channel 2 of the ADC. The sampling and field modulation waveforms are phase-locked via generation by a common arbitrary waveform generator (AWG). An output from the AWG indicating the periodic zero-crossing of the field modulation waveform is also fed to the ADC (connection iii in Fig. 3). This signal encodes the true phase of the field modulation, and is used to synthetically generate a field modulation waveform and its harmonics; the individual harmonics of the EPR spectrum are extracted by matched filtering S_I and S_Q with the synthetically generated field modulation waveforms. Traditional AFC circuitry [17], employing PSD, is used to lock ω_c to the resonant frequency of the cavity, ω_0 . The time-constant of the AFC is kept large enough to ensure that there is no AFC response to ω_m or any of its multiples. Typical design parameters for the digital receiver are summarized in Table 1, and specifications of the major components are reported in Table 2.

No reference arm was used in our design. Since the reference signal (C_1) was not fed to the AFC diode, the design solely relied on the reflected microwave energy in C_2 to bias the diode. To ensure an adequate energy in C_2 for biasing, the spectrometer was operated under suboptimal condition of either overcoupling or undercoupling. Too much departure from the critical coupling ($\beta_0 = 1$), however, was troublesome in a number of ways. First, it decreased the overall sensitivity of the system. Second, it threatened to saturate the LNA. Lastly, it reduced the effective vertical resolution of the ADC because the EPR signal became increasingly smaller than the dynamic range of the ADC defined by the stronger microwave carrier. Therefore, the coupling was kept as close to the critical value as allowed by the AFC locking capability. However, the requirement of over or undercoupling can be avoided altogether by using a different AFC design. For example, a quadrature



Fig. 1. Frequency domain illustration of digital detection. Reflected EPR signal along with the noise shown in gray (i); reflected signal after bandpass filtering (ii); sampling frequency generated by AWG (iii); sampled bandpass reflected signal (iv); sampled bandpass microwave signal from the microwave source (v); baseband signal S_i (or S_Q , depending on the phase of microwave signal) obtained by point-by-point time-domain multiplication of iv and v (vi); sampled field modulation signal (vii); point-by-point time-domain multiplication of iv and v (vi); sampled field modulation signal (vii); digital lowpass filtering to obtain one sample of the I_1 (or Q_1) (ix). For simplicity, only one harmonic is displayed around the microwave carrier.

AFC design with its own phase-insensitive reference arm [25] can handle this shortcoming.

Unlike time-locked subsampling [19], a strict adherence to ω_s values that generate four samples in an odd number of cycles is not required in our design. Any value of ω_s that result in nonoverlapping replicas of the bandpass microwave signal is a viable option. Although it is possible to use lower sampling frequency, a higher frequency, even when it is below the Nyquist rate, offers advantages. The most important benefit of a high sampling rate is its positive effect on the antialiasing bandpass filter design. A large value of ω_s alleviates the requirement of sharp transition from pass-band to stop-band. Also, it allows for filters with lower quality-factor, which are easier to design and possess favorable characteristics such a uniform amplitude and group delay across the bandwidth of the EPR signal. Another advantage of high ω_s is the increase in effective vertical resolution of the ADC [26]. The only downside of a high sampling frequency is the amount of data generated. For our design, the two ADC channels collectively generated 6 GB of data for a four second scan. Although the PCI express-based ADC board itself is capable of real-time streaming, the actual data transfer from the ADC on-board memory to the computer took 40 s, primarily due to slow write speed of the hard drive. This limitation, however, can be overcome by using commercially available fast storage systems. For example, PCI express host adapter (ExpressSAS H6F0) by Atto Technology (Amherst, New

York) is capable of handling up to 600 MB/s bandwidth for each of its 16 external ports.

2.3. Signal and noise model

Phase noise, defined by the random additive variations in the phase of the microwave signal, is invariably present in the output of any oscillator. Depending on the type of resonator, type of oscillator, and microwave power, the phase noise may become the dominant noise source in the EPR spectra. Several solutions have been proposed by the EPR community to counter the effects of phase noise. Some common remedies include: avoiding the phase noise prone dispersion component altogether; using a low-phase noise Gunn diode oscillator [27]; using a low quality-factor loop-gap resonator [18]; reducing the incident microwave power; and using a bimodal resonator [28,29]. Our approach does not eliminate or suppress the phase noise itself, but instead exploits a quadrature receiver to reliably estimate EPR lineshape parameters in the presence of phase noise. Also, the approach, which is capable of handling unknown microwave phase, is an attractive alternative to adjusting the phase by manual tuning [30].

Because the two inputs arriving at the ADC are not phaselocked, the harmonics generated by the S_I and S_O channels are



Fig. 2. Block diagram of CW spectrometer capable of direct digital detection.

not purely absorption and dispersion but instead are a combination given by

$$I_{h}(H_{0}) = a_{h}(H_{0}) \cos \phi_{0} - b_{h}(H_{0}) \sin \phi_{0}$$

$$Q_{h}(H_{0}) = a_{h}(H_{0}) \sin \phi_{0} + b_{h}(H_{0}) \cos \phi_{0}$$
(1)

where H_0 represents the external magnetic field; ϕ_0 denotes the unknown microwave phase discrepancy between the two channels of the ADC; I_h and Q_h represent the *h*th harmonic extracted from S_I and S_Q , respectively; and $a_h(H_0)$ and $b_h(H_0)$ represent absorption and dispersion lineshapes [6] for the *h*th harmonic.

In the presence of noise, including phase noise, Eq. (1) can be modified to

$$I_{h}(H_{0}) = a_{h}(H_{0})\cos\phi_{0} - (b_{h}(H_{0}) + p)\sin\phi_{0} + u$$

$$Q_{h}(H_{0}) = a_{h}(H_{0})\sin\phi_{0} + (b_{h}(H_{0}) + p)\cos\phi_{0} + v$$
(2)

where *p* represents phase noise and has uncorrelated zero-mean Gaussian entries with variance σ_p^2 . The sampled noise values in *u* and *v* represent collective noise from all other sources (primarily amplifiers) in the in-phase and out-of-phase channels, respectively. Both *u* and *v* are independent and identically distributed Gaussian [11] random variables with variance σ_0^2 . For the derivation of Eq.



Fig. 3. Basic layout for a digital receiver. Sampling signal (i); field modulation waveform (ii); trigger indicating the zero-crossing of the field modulation waveform (iii); reflected EPR signal to channel 1 of the ADC (iv); microwave signal to channel 2 of ADC (v); trigger from the Bruker (Billerica, MA) field controller to initiate data acquisition (vi); and sampled channel 1 (C_1), sampled channel 2 (C_2), and sampled trigger for the field modulation (vii).

Table 1	
Typical parameter values for the designed L-band digital receiver.	

Parameter	Symbol	Value
Microwave frequency Sampling frequency Modulation frequency AFC frequency Microwave power	ω_c ω_s ω_m	$2\pi \times 1.283 \times 10^9 \text{ rad/s}$ $2\pi \times 400 \times 10^6 \text{ rad/s}$ $2\pi \times 100 \times 10^3 \text{ rad/s}$ $2\pi \times 76.8 \times 10^3 \text{ rad/s}$ 2 mW

(2), see Appendix A. For $\phi_0 = 0$, Fig. 4 shows Cramér–Rao lower bound (CRLB) and corresponding simulation results displaying the impact of collecting multiple harmonics on the estimation error of full-width half-maximum (FWHM) linewidth τ for varying degrees of phase noise.

The digital receiver considered here provides quadrature detection with respect to the microwave phase but only a single-channel (in-phase) detection with respect to the field modulation phase. Under nonsaturating conditions, the out-of-phase field modulation channel contains negligible energy and hence can be ignored.

2.4. Parameter estimation

For the spectroscopic data, the unknown parameters include linewidth τ , spin density d, microwave phase ϕ_0 , baseline offset (one per each harmonic component), baseline slope (one per each harmonic component), center field, and modulation amplitude H_m . For $\phi_0 \neq 0$, the absorption (a_h) and dispersion (b_h) components get mixed (Eq. (2)) and so does the phase noise. If σ_p^2 is not negligible compared to σ_0^2 , the contamination from phase noise can adversely affect the SNR of both I_h and Q_h components. Therefore, in order to best estimate linewidth, it is important to estimate and adjust the nuisance parameter ϕ_0 .

In this work, we have adopted a postprocessing approach, termed as iterative phase-rotation estimation (IPRE), to compute the unknown parameters by jointly processing the multiple harmonics. A pseudo code for the IPRE implementation is as follows:

Initialization:

$$\phi_0^{(0)} = 0$$

$$C_2^{(0)} = C_2$$

Table 2Digital receiver components specifications.

Component	Vendor and specification
BPF LNA ADC	K & L Microwave (custom made), center = $2\pi \times 1.282 \times 10^9$ rad/s, bandwidth = $2\pi \times 75 \times 10^6$ rad/s HD Communications (HD 24410), gain = 40 dB Ultraview Corp. (AD12-500 × 2–8 GB), upto 500 MS/s, 12 bit vertical resolution, and 8 GB RAM
Resonator Oscillator Field controller AWG Computer	Home built reentrant resonator, 12 mm diameter, 12 mm length, $\omega_0 = 2\pi \times 1.283 \times 10^9$ rad/s Englemann microwave (CC-12), cavity oscillator, $\omega_c = 2\pi \times (1-2) \times 10^9$ rad/s Bruker ER 032M Tektronix (AWG7122B) Ultraview Corp., Intel dual core 2.66 GHz, 8 GB RAM, 1 TB hard drive



Fig. 4. Simulation (dotted line) and CRLB (solid line) results showing the impact of multiple harmonics with (gray) and without (black) the phase noise. FWHM linewidth τ = 1 G and field modulation amplitude H_m = 1 G (a) and H_m = 3 G (b). For each parameter set, 500 trial runs are considered for the simulation.

Iteration:

$$C_{2}^{(j)} = \text{ROT}(C_{2}^{(j-1)}, \phi_{0}^{(j-1)})$$

$$S_{I}^{(j)} = C_{1}C_{2}^{(j)}$$

$$S_{Q}^{(j)} = C_{1}\check{C}_{2}^{(j)}$$

$$I_{h}^{(j)} = \text{MF}(S_{I}^{(j)}, h\omega_{m})$$

$$Q_{h}^{(j)} = \text{MF}(S_{Q}^{(j)}, h\omega_{m})$$

$$\{\phi_{0}^{(j)}, \tau^{(j)}, d^{(j)}\} = \text{WLS}(I_{h}^{(j)}, Q_{h}^{(j)})$$
end

where ROT($C_2^{(j-1)}, \phi_0^{(j-1)}$) represents phase-rotation of $C_2^{(j-1)}$ by $\phi_0^{(j-1)}$, MF represents digital matched filtering, WLS represents weighted least-squares curve fitting, and j indicates the iteration number. Note, for $\phi_0^{(0)} = 0$, $C_2^{(1)} = C_2^{(0)} = C_2$.

In the first iteration of the IPRE, a weighted least-squares curve fitting is performed on the quadrature harmonics, $I_h^{(1)}$ and $Q_h^{(1)}$, extracted from the original data C_1 and C_2 . The estimated microwave phase from iteration 1 is denoted by $\phi_0^{(1)}$. In the second iteration, $C_2^{(1)}$ is rotated by $\phi_0^{(1)}$, and this phase-rotated version of C_2 is denoted by $C_2^{(2)}$. Both $S_l^{(2)}$ and $S_Q^{(2)}$ are reconstructed by multiplication of C_1 with phase-rotated $C_2^{(2)}$ and $S_Q^{(2)}$ are matched filtered with the



Fig. 5. Impact of collecting two channels for $\sigma_p^2 = 0$ (a) and for $\sigma_p^2 = 20\sigma_0^2$ (b). First six harmonics are considered for $\tau = 1$ G and $H_m = 1$ G for both single-channel and quadrature estimations. Five hundred trial runs are considered for every one degree increment in ϕ_0 .

synthetically generated modulation waveform and its harmonics. The iterative process is repeated until a convergence criterion is reached.

When $\phi_0^{(j)}$ approaches zero, the corresponding $I_h^{(j)}$ and $Q_h^{(j)}$ approximate pure absorption and dispersion lineshapes of the *h*th harmonic, respectively. In each iteration, the curve fitting is performed using nonlinear weighted least-squares, with weighting of $I_h^{(j)}$ and $Q_h^{(j)}$ proportional to $1/\sqrt{\sigma_0^2 + \sigma_p^2 \sin^2 \phi_0^{(j)}}$ and $1/\sqrt{\sigma_0^2 + \sigma_p^2 \cos^2 \phi_0^{(j)}}$, respectively. Since the true values of σ_0^2 and σ_p^2 may not be known, approximate values can be estimated from the tails of the Fourier transform of $I_h^{(j)}$ and $Q_h^{(j)}$. Alternatively, the process of least-squares can be performed twice within each iteration, such that $\hat{\sigma}_0^2$ and $\hat{\sigma}_p^2$ estimated from the residuals of the first unweighted least-squares curve fitting are used in the second weighted least-squares curve fitting.

For the simulation and experimental studies reported in this work, we terminated the IPRE after only two iterations. We observed a very rapid convergence of the IPRE, and increasing the number of iterations beyond two did not provide further improvement. For cases where slow convergence is expected, for example in extremely low SNR, it is possible to increase the number of iterations. The parameters estimated by the IPRE are locally convergent to a maximum-likelihood estimate for the signal model in Eq. (1). Although it is possible to phase-rotate the reconstructed harmonics I_h and Q_h directly, such a procedure would only further mix the various noise terms and generate a suboptimal solution.

3. Results

3.1. Simulation

The purpose of this simulation study is to establish the benefit of quadrature detection in comparison to the previously reported single channel detection [22]. For $\sigma_p^2 \ll \sigma_0^2$, adding the second channel provides approximately 3 dB SNR gain irrespective of the ϕ_0 value. On the other hand, for phase noise power σ_p^2 which is comparable to or larger than σ_0^2 , the benefit of adding a second channel lies not in an explicit 3 dB gain in SNR but rather in the ability to accurately estimate ϕ_0 . Even a small ϕ_0 , if unaccounted, can result in a degraded estimation of τ . Fig. 5 compares the performance of a quadrature receiver with that of a single-channel receiver, for varying values of ϕ_0 . For a single-channel receiver, a complex Lorentzian signal model [31] was used to estimate τ , while for a quadrature receiver the proposed IPRE was used for the estimation.

3.2. L-band spectroscopy

A spectroscopy experiment was conducted on an L-band system equipped with the proposed digital receiver. The related parameters of the system are reported in Tables 1 and 2. The sample was made from a single small crystal of LiNc-BuO [32] sealed in a capillary tube under anoxic conditions. A previously measured anoxic τ was observed to be 0.658 G.

Two datasets were collected with nominal field modulation values of 0.25 G and 2.0 G, respectively. After two iterations of the IPRE, the actual field modulation values were found to be 0.27 G and 2.08 G, respectively. Each dataset was comprised of 12 repeated identical scans. The scan time was 3.9 s with a sweep width of 10 G. Fig. 6 shows the effect of microwave phase-rotation on I_h and Q_h harmonics. Fig. 7 shows the fitting results from iteration 2 of the IPRE. Fig. 8 displays the noise correlation between $I_h^{(1)}$ and $Q_h^{(1)}$ and also between $I_h^{(2)}$ and $Q_h^{(2)}$. Fig. 9 compares the standard deviation of estimated τ based



Fig. 6. In-phase (*I_h*) and out-of-phase (*Q_h*) harmonics before (a) and after (b) the second iteration of the IPRE. From left to right, four harmonics are shown for *H_m* = 2.08 G. The data were collected on an L-band CW spectrometer equipped with the proposed digital receiver. The dashed-line indicates *x*-axis.



Fig. 7. The fitted curves $\tilde{I}_{b}^{(2)}$ and $\tilde{Q}_{b}^{(2)}$ and the two times magnified residuals corresponding to Fig. 6b.



Fig. 8. Impact of C_2 phase-rotation on the correlation of noise across I_h and Q_h . Noise cross-correlation between $I_1^{(1)}$ and $Q_1^{(1)}$ (a) and between $I_1^{(2)}$ and $Q_1^{(2)}$ (b) computed from the residuals shown in the Fig. 7.



Fig. 9. Impact of collecting multiple harmonics on standard error of τ estimation. The experiment was conducted on a L-band CW EPR system equipped with the proposed quadrature digital receiver. Twelve scans were collected for each modulation amplitude.

on first harmonic with the estimation based on the first four harmonics.

4. Discussion

The phase noise, originating from the microwave source, does not affect the absorption and dispersion equally. The frequency fluctuations due to phase noise enter as a first-order effect for the dispersion and a second-order effect for the absorption [33]. Therefore, when present in moderation, the phase noise manifests itself almost exclusively in the dispersion. The noise from the other sources, such as the noise from the LNA and the thermal noise from the resonator, however, tends to affect both absorption and dispersion equally. Therefore, for the noise model considered (Eq. (2)), I_h and Q_h components have equal and independent noise terms, u and v respectively, as well as a shared noise term, p, arising from the phase noise.

The relocation of phase noise exclusively to the out-of-phase channel requires knowledge of the microwave phase, ϕ_0 . The digital detection, with its retrospective digital data processing

capabilities, allows for an accurate estimation and compensation of ϕ_0 , eliminating the requirement of manual tuning or additional hardware development. The proposed IPRE relocates the phase noise to the out-of-phase channel by iteratively estimating ϕ_0 and phase-rotating C2. Fig. 5 compares, for the simulated data, the performance of a quadrature receiver and the IPRE processing to that of a signal-channel receiver. Fig. 5a suggests an approximately 3 dB gain in SNR for adding the second channel when the phase noise is negligible. For cases with considerable phase noise, Fig. 5b shows a microwave phase-independent performance of the IPRE as compared to a single-channel detection whose performance heavily relies on the ϕ_0 value. Different selections of τ and H_m yielded similar trends. For the simulation, we chose $\sigma_n^2 = 20\sigma_0^2$ because in the preliminary testing of our digital receiver we consistently encountered σ_p^2 values which were 10–20 times σ_0^2 depending on the microwave power level.

Fig. 6 displays one of the measured datasets before and after the second iteration of IPRE, highlighting the transfer of the phase noise from the in-phase to the out-of-phase channel. For the dataset shown in Fig. 6, the noise variances were 5.06×10^{-4} and 8.95×10^{-4} in $I_1^{(1)}$ and $Q_1^{(1)}$, respectively, and 1.60×10^{-4} and 12.2×10^{-4} in $I_1^{(2)}$ and $Q_1^{(2)}$, respectively. Fig. 8 displays the noise correlation, computed from residuals of the curve fitting, after the first and second iterations of the IPRE. A considerable decrease in the correlation is a direct consequence of $\phi_0^{(2)} \approx 0$. The cross-correlation shows the noise is uncorrelated across time, in support of the model in Eq. (2). Additionally, the zero-lag noise correlation between the I_h and Q_h components shows marked decrease after one iteration of the IPRE, illustrating proper rotation of the microwave phase to yield the Q_h components as purely dispersion. For the experimental data, the estimated value of $\phi_0^{(2)}$ in degrees was 0.026 ± 0.38 .

Fig. 9 illustrates the benefit of collecting multiple harmonics. The standard error of estimation based on the first four harmonics is 29% lower than that of first harmonic alone collected at 2.08 G field modulation, which translates to approximately 50% reduction in the acquisition time. Further speed up is possible by considering more harmonics and by optimizing the field modulation amplitude. As expected, adding more harmonics for small H_m does not improve the estimation of τ while for high H_m the estimation of τ progressively improves by using more harmonics.

All postprocessing was performed in Matlab (Mathorks, MA) on a computer equipped with 2.66 GHz dual core Intel CPU, 8 GB RAM, and 64-bit CentOS operating system. The sampled data, C_1 and C_2 , from each scan were decomposed into 1024 data blocks with each block corresponding to 38 ms of scan time. A decomposition into 4096 blocks (data not shown) produced similar results. The reconstruction of four absorption and four dispersion harmonics, which involved two iterations of the IPRE, took nearly 35 min. Because the computationally expensive processing is conducted block-by-block, parallelization of the implementation is trivial. Likewise, use of a field programmable gate array can accelerate the processing. In the presence of the AFC and field modulation, the instantaneous frequency of C₂ continuously varied along the scan, making the synthesis of a potentially cleaner digital version of C_2 difficult. We observed that using experimentally observed C_2 instead of a digitally estimated replica tone produced better results.

The baseline drift, possibly due to microphonics, was most prominent in the first harmonic. The problem was handled by estimating two unknowns, one for the offset and one for the slope, for each harmonic component. Also, the other nuisance parameters of field modulation amplitude and center field were likewise jointly estimated with the parameters of interest, i.e., linewidth and spin density.

5. Conclusions

A quadrature digital receiver and associated signal estimation procedure are reported for L-band EPR spectroscopy. The data acquisition and processing of multiple harmonics in both in-phase and out-of-phase channels are presented. The receiver allows direct digital down-conversion, with heterodyne processing using digital capture of the microwave reference signal. Thus, the receiver avoids noise and nonlinearity associated with analog mixers. The retrospective signal processing is suitable for arbitrary microwave phase and arbitrary levels of oscillator phase noise. The proposed processing scheme is applicable for Lorentzian lineshape under nonsaturating conditions but can be extended to other parametric families of lineshapes. Simulation and experimental data illustrate the application and relative merits of our design. For the settings shown, the receiver provided 50% reduction in acquisition time when comparing results from first four harmonics to those of first harmonic alone. Even higher accelerations, under different parameter settings, are possible.

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Appendix A

Here, we develop a simple noise model for field modulated CW EPR spectra. This model is particularly useful when contributions of phase noise originating from the microwave source, in comparison to contributions from other sources of noise, are not negligible. While developing this model we have made following assumptions: (i) the phase noise is additive, i.e., it can be represented by adding a random process to the phase of the microwave signal; (ii) all other sources of noise can be represented by adding random processes to the signals from the circulator and the microwave source; (iii) frequency fluctuations of the source due to phase noise are comparable to or smaller than the frequency fluctuations due to the magnetic resonance; (iv) magnetic field value varies slowly and can be approximated by a constant across each data block; and (v) oscillator phase noise spectrum is centered around ω_c and is bandlimited [34] with a bandwidth $\ll \tilde{\omega}_c$, with $\tilde{\omega}_c$ defined later in appendix. This noise model, along with the Robinson-Mailer model [6] that defines the EPR lineshape in the presence of field modulation, is then used in a weighted leastsquares curve fitting of the measured EPR data.

The majority of CW EPR spectrometers employ a reflection cavity. The microwave signal reflected from the sample cavity encodes the EPR information. A change in complex magnetic susceptibility χ , due to magnetic resonance, changes the reflection coefficient Γ of the cavity, creating a small change in the amplitude and phase of the reflected power. This variation in the reflected signal, upon detection, is converted to an EPR signal. The reflection coefficient, in the absence of magnetic resonance, can be expressed as,

$$\Gamma_0 = \frac{1 - \beta_0 - j\xi_0}{1 + \beta_0 - j\xi_0} \tag{A.1}$$

where coupling parameter β_0 and normalized frequency mismatch ξ_0 are defined as [35]

$$\begin{aligned} \beta_0 &= \frac{q_0}{q_T} \\ \xi_0 &= -q_0 \left(\frac{\omega_c}{\omega_0} - \frac{\omega_0}{\omega_c} \right) \\ &\approx 2q_0 \left(\frac{\omega_0 - \omega_c}{\omega_0} \right) \end{aligned} \tag{A.2}$$

In the above expression, the unloaded quality-factor, q_0 , is proportional to the ratio of the energy stored in the cavity to the energy lost in the cavity; the radiation quality-factor, q_T , is proportional to the ratio of energy stored in the cavity to the energy lost into the transmission line; ω_c represents the frequency of the oscillator (microwave source); ω_0 represents the resonant frequency of the cavity; and subscript "0" indicates that the value is observed in the absence of magnetic resonance.

Upon magnetic resonance, a change in the imaginary component of magnetic susceptibility $\Delta \chi_i$ translates to a change in q_0 , giving rise to the absorption signal, while a change in the real component of magnetic susceptibility $\Delta \chi_r$ translates to a change in ω_0 , generating the dispersion signal. Therefore, in the presence of magnetic resonance, which varies with the external magnetic field H_0 , we get [35],

$$q(H_0) = q_0 - \eta q_0^2 \Delta \chi_i(H_0)$$

$$\omega(H_0) = \omega_0 - \frac{\eta}{2} \omega_0 \Delta \chi_r(H_0)$$
(A.3)

where $\Delta \chi_i(H_0)$ and $\Delta \chi_r(H_0)$ are connected by Kramers–Kronig relation and describe the absorption and dispersion components of EPR spectrum. In the presence of magnetic resonance, Eqs. (A.1) and (A.2) can be written as,

$$\begin{split} \beta(H_0) &= \frac{q(H_0)}{q_T} \\ \xi(H_0) &= 2q_0 \left(\frac{\omega(H_0) - \omega_c}{\omega(H_0)} \right) \\ \Gamma(H_0) &= \frac{1 - \beta(H_0) - j\xi(H_0)}{1 + \beta(H_0) - j\xi(H_0)} \end{split} \tag{A.4}$$

For brevity, we will use β , ξ , and ω to represent $\beta(H_0)$, $\xi(H_0)$, and $\omega(H_0)$, respectively.

From Eqs. (A.1) and (A.4), the real part of $\Gamma(H)$ can be expressed as

$$\Gamma_r(H_0) = \frac{1 - \beta^2 + (2q_0(\omega - \omega_c)/\omega)^2}{(1 + \beta)^2 + (2q_0(\omega - \omega_c)/\omega)^2}$$
(A.5)

which in the presence of additive phase noise [36], $\phi(t)$, becomes,

$$\Gamma_{r,\phi}(H_0,t) = \frac{1 - \beta^2 + (2q_0(\omega - \omega_c - \Delta\omega_c(t))/\omega)^2}{(1 + \beta)^2 + (2q_0(\omega - \omega_c - \Delta\omega_c(t))/\omega)^2}$$
(A.6)

where $\Delta\omega_c(t) = d(\phi(t))/dt$ is the equivalent frequency noise defined as the variation in the instantaneous frequency ω_c of the microwave signal. In terms of the Taylor series with respect to $\Delta\omega_c(t)/\omega$, we can write

$$\Gamma_{r,\phi}(H_0,t) = \Gamma_{r,\phi}(H_0,t)|_{\frac{\Delta\omega_c(t)}{\omega} = 0} + \frac{\Delta\omega_c(t)}{\omega} \frac{\partial}{\partial t} (\Gamma_{r,\phi}(H_0,t))|_{\frac{\Delta\omega_c(t)}{\omega} = 0} + O\left(\left(\frac{\Delta\omega_c(t)}{\omega}\right)^2\right)$$
(A.7)

By neglecting the higher order terms, denoted by $O(\cdot)$, Eq. (A.7) can be simplified to

$$\Gamma_{r,\phi}(H_0,t) \approx \Gamma_r(H_0) + \frac{8\beta(1+\beta)\xi q_0}{(1+\beta)^2 + \xi^2} \frac{\Delta\omega_c(t)}{\omega}$$
(A.8)

For values of $|\Delta\omega_c|$ which are comparable to or smaller than max{ $|\omega-\omega_c|$ }, the second term on the right hand side of Eq. (A.8) is negligible compared to the maximum variation, due to magnetic resonance, in the first term for typical parameter values for an L-band spectrometer. Therefore, Eq. (A.8) can be approximated by

$$\Gamma_{r,\phi}(H_0,t) \approx \Gamma_r(H_0) \tag{A.9}$$

For dispersion, an expression equivalent to Eq. (A.6) can be written as

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$$\Gamma_{i,\phi}(H_0,t) = \frac{-4\beta_0 q_0(\omega - \omega_c - \Delta\omega_c(t))/\omega}{(1+\beta)^2 + (2q_0(\omega - \omega_c - \Delta\omega_c(t))/\omega)^2}$$
(A.10)

Approximating Eq. (A.10) with the first two terms of the Taylor series with respect to $\Delta \omega_c(t)/\omega$ yields,

$$\Gamma_{i,\phi}(H_0,t) \approx \Gamma_i(H_0) + \frac{4\beta q_0 ((1+\beta)^2 - \xi^2)}{((1+\beta)^2 + \xi^2)^2} \frac{\Delta \omega_c(t)}{\omega}$$
(A.11)

For values of $|\Delta\omega_c|$ which are comparable to max{ $|\omega-\omega_c|$ }, the second term on the right hand side of Eq. (A.11) is not negligible when compared to the maximum variation, due to magnetic resonance, in the first term for typical parameter values for an L-band spectrometer. Therefore, Eq. (A.11) can be approximated by

$$\Gamma_{i,\phi}(H_0,t) \approx \Gamma_i(H_0) + k_1 \Delta \omega_c(t) \tag{A.12}$$

where constant $k_1 = 4\beta_0 q_0/(\omega_0(1 + \beta_0)^2)$.

The reflection coefficient affects both magnitude and phase of the reflected microwave signal. The real part Γ_r generates the inphase (with respect to the incident microwave phase) component and the imaginary part Γ_i generates the out-of-phase component of the reflected signal C_1 . Therefore, we can write,

$$C_{1}(H_{0},t) = \Gamma_{r,\phi}(H_{0},t)\cos(\omega_{c}t + \phi(t)) + \Gamma_{i,\phi}(H_{0},t)\sin(\omega_{c}t + \phi(t))$$
(A.13)

Here, without the loss of generality, the incident microwave signal is assumed to be of unit peak amplitude.

Phase noise is not the only source of noise present. Other sources of noise, such as noise from the amplifiers, are also present. We represent all other noise sources by an added term $z_1(t)$.

$$C_1(H_0, t) = \Gamma_{r,\phi}(H_0, t) \cos(\omega_c t + \phi(t)) + \Gamma_{i,\phi}(H_0, t)$$

$$\times \sin(\omega_c t + \phi(t)) + z_1(t)$$
(A.14)

In digital detection, only the sampled version of the signal is available. If the sampling frequency ω_s does not meet the Nyquist criteria then the signal C_1 is copied at $\{\omega_c - N\omega_s\}$ for all integers *N*. For a bandpass signal, however, bandpass filtering and a proper selection of ω_s ensures that the subsampling does not generate aliasing artifacts, yielding,

$$C_{1}[H_{0}, n] = \Gamma_{r,\phi}[H_{0}, n] \cos(\tilde{\omega}_{c}n + \phi) + \Gamma_{i,\phi}[H_{0}, n] \\ \times \sin(\tilde{\omega}_{c}n + \phi) + z_{1}[n]$$
(A.15)

where $\tilde{\omega}_c = \min\{|\omega_c - N\omega_s|\}$ with $N = 0 \pm 1 \pm 2 \cdots$, n = mT with $m = 0 \pm 1 \pm 2 \cdots$, and *T* is the sampling interval.

To obtain in-phase and out-of-phase baseband signals, the reflected sampled signal C_1 is multiplied with the microwave source signal C_2 and its Hilbert transform. Like C_1 , the signal C_2 is also bandpass filtered and sampled at ω_s . If S_1 and S_Q represent the in-phase and out-of-phase channels, we can write

$$S_{I}[H_{0}, n] = C_{1}[H_{0}, n]C_{2}[H_{0}, n]$$

= $C_{1}[H_{0}, n] \left(\cos \left(\tilde{\omega}_{c} n + \phi_{0} + \tilde{\phi}[n] \right) + z_{2}[n] \right)$
= $\frac{1}{2} (\Gamma_{r}(H_{0}) \cos(\phi_{0} + \Delta \phi[n]) + g_{I}[n] - (\Gamma_{i}(H_{0}) + k_{1} \Delta \omega_{c}[n]) \sin(\phi_{0} + \Delta \phi[n])) + z_{I}[n]$ (A.16)

where $z_2[n]$ represents additive noise in C_2 , $g_l[n]$ represent higher frequency terms, $z_l[n]$ represents a composite noise term which is the summation of all terms involving $z_1[n]$ and $z_2[n]$, and $\tilde{\phi}[n]$ is the time-delayed version of $\phi[n]$, and $\Delta\phi[n] = \tilde{\phi}[n] - \phi[n]$. Using truncated power series, Eq. (A.16) can be approximated by,

$$S_{I}[H_{0}, n] \approx \frac{1}{2} (\Gamma_{r}(H_{0})(\cos \phi_{0} - \Delta \phi[n] \sin \phi_{0}) + g_{I}[n] - (\Gamma_{i}(H_{0}) + k_{1} \Delta \omega_{c}[n])(\sin \phi_{0} + \Delta \phi[n] \cos \phi_{0})) + z_{I}[n]$$
(A.17)

Usually $\Delta \phi[n]$ is negligible, especially for time correlated frequency noise, as compared to the $k_1 \Delta \omega_c[n]$ term. However, for overcoupling $\beta_0 > 1$ and undercoupling $0 < \beta_0 < 1$, a considerable fraction of microwave energy is reflected back which dwarfs the small variations in the reflected energy due to magnetic resonance. Since $\omega_c \approx \omega_0$ for systems equipped with AFC, $\Gamma_r[H_0,n] \gg \Gamma_i[H_0,n]$ and $\Gamma_r[H_0,n] \approx \frac{1-\beta_0}{1+\beta_0}$. For such cases, the term $\Gamma_r[H_0,n] \Delta \phi[n] \sin \phi_0$ may not be negligible and $S_I[H_0,n]$ becomes,

$$S_{I}[H_{0}, n] \approx \frac{1}{2} \Gamma_{r}(H_{0})(\cos \phi_{0} - (\Gamma_{i}(H_{0}) + k_{1}\Delta\omega[n] + k_{2}\Delta\phi[n]) \\ \times \sin \phi_{0}) + g_{I}[n] + z_{I}[n] \\ = \frac{1}{2} (\Gamma_{r}(H_{0})\cos \phi_{0} - (\Gamma_{i}(H_{0}) + k[n])\sin \phi_{0}) + g_{I}[n] + z_{I}[n]$$
(A.18)

where $k_2 = \frac{1-\beta_0}{1+\beta_0}$, and $k[n] = k_1 \Delta \omega_c[n] + k_2 \Delta \phi[n]$ represents the phase noise. We can write an equivalent expression for the out-of-phase channel S_Q ,

$$S_{Q}[H_{0}, n] = C_{1}[H_{0}, n] \breve{C}_{2}[H_{0}, n]$$

= $\frac{1}{2} (\Gamma_{r}(H_{0}) \sin \phi_{0} + (\Gamma_{i}(H_{0}) + k[n]) \cos \phi_{0})$
+ $g_{Q}[n] + z_{Q}[n]$ (A.19)

where \check{C}_2 represents the Hilbert transform of C_2 , $g_Q[n]$ and $z_Q[n]$ are equivalent to $g_l[n]$ and $z_l[n]$. For a phase noise with bandwidth $\ll \tilde{\omega}_c$, the microwave phase varies gradually with time, and hence C_2 maintains its local fidelity to a sinusoid. Therefore, $\check{C}_2 \approx \sin(\tilde{\omega}_c n + \phi_0 + \tilde{\phi}[n]) + \check{z}_2[n]$

In the case of field modulation, with amplitude H_m and frequency ω_m , we can write $H[n] \equiv H_0 + H_m \cos \omega_m n$. The process of harmonic extraction is done block-by-block, i.e., the incoming data are broken down to smaller blocks each corresponding to a fixed H_0 and the each block is digitally matched filtered with $\cos(\omega_m n)$ and its harmonics. The *h*th harmonic can be extracted by,

$$I_{h}[H_{0}] = \sum_{n} S_{I}(H[n]) \cos(h\omega_{m}n)$$

= $\frac{1}{2} \cos \phi_{0} \sum_{n} \Gamma_{r}(H[n]) \cos(h\omega_{m}n) - \frac{1}{2} \sin \phi_{0}$
 $\times \sum_{n} (\Gamma_{i}(H[n]) \cos(h\omega_{m}n) + k[n] \cos(h\omega_{m}n)) + \frac{1}{2}$
 $\times \sum_{n} z_{I}[n] \cos(h\omega_{m}n) + \frac{1}{2} \sum_{n} g_{I}[n] \cos(h\omega_{m}n)$ (A.20)

where the summation is performed over each data block. For a large enough block size, the contamination from the $g_i[n]$ terms can be neglected. By defining,

$$a_{h}(H_{0}) \equiv \frac{1}{2} \sum_{n} \Gamma_{r}(H[n]) \cos(h\omega_{m}n)$$

$$b_{h}(H_{0}) \equiv \frac{1}{2} \sum_{n} \Gamma_{i}(H[n]) \cos(h\omega_{m}n)$$

$$p(H_{0}) \equiv \frac{1}{2} \sum_{n} k[n] \cos(h\omega_{m}n)$$

$$u(H_{0}) \equiv \frac{1}{2} \sum_{n} z_{I}[n] \cos(h\omega_{m}n)$$

$$v(H_{0}) \equiv \frac{1}{2} \sum_{n} z_{Q}[n] \cos(h\omega_{m}n)$$
(A.21)

the expression for in-phase, (*I*), and out-of-phase, (*Q*), harmonics can be simplified as,

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$$\begin{aligned} &I_h(H_0) = a_h(H_0)\cos\phi_0 - (b_h(H_0) + p)\sin\phi_0 + u\\ &Q_h(H_0) = a_h(H_0)\sin\phi_0 + (b_h(H_0) + p)\cos\phi_0 + \upsilon \end{aligned} \tag{A.22}$$

References

- S.S. Eaton, G.R. Eaton, L.J. Berliner (Eds.), Biomedical EPR, Part A: Free Radicalsm, Metals, Medicine and Physiology, Kluwer Academic, New York, 2004.
- [2] H. Swartz, In Vivo EPR (ESR): Theory and Applications, Kluwer Academic, New York, 2003.
- [3] M. Elas, R. Bell, D. Hleihel, E. Barth, C. McFaul, C. Haney, J. Bielanska, K. Pustelny, K. Ahn, C. Pelizzari, M. Kocherginsky, H. Halpern, Electron paramagnetic resonance oxygen image hypoxic fraction plus radiation dose strongly correlates with tumor cure in FSa fibrosarcomas, Int. J. Radiat. Oncol. Biol. Phys. 71 (2008) 542–549.
- [4] R. Ahmad, P. Kuppusamy, Theory, instrumentation, and applications of electron paramagnetic resonance oximetry, Chem. Rev. (2010) 3212–3236.
- [5] S. Subramanian, M. Krishna, Dancing with the electrons: time-domain and CW in vivo EPR imaging, Magn. Reson. Insights 2 (2008) 43-74.
- [6] B. Robinson, C. Mailer, A. Reese, Linewidth analysis of spin labels in liquids: I. Theory and data analysis, J. Magn. Reson. 138 (1999) 199–209.
- [7] H. Sato-Akaba, Y. Kuwahara, H. Fujii, H. Hirata, Half-life mapping of nitroxyl radicals with three-dimensional electron paramagnetic resonance imaging at an interval of 3.6 s, Anal. Chem. 81 (2009) 7501–7506.
- [8] J. Joshi, J. Ballard, G. Rinard, R. Quine, S. Eaton, G. Eaton, Rapid-scan EPR with triangular scans and Fourier deconvolution to recover the slow-scan spectrum, J. Magn. Reson. 175 (2005) 44–51.
- [9] R. Quine, G. Rinard, S. Eaton, G. Eaton, A pulsed and continuous wave 250 MHz electron paramagnetic resonance spectrometer, Concepts Magn. Reson. 15 (2002) 59–91.
- [10] S. Subramanian, K. Matsumoto, J. Mitchell, M. Krishna, Radio frequency continuous-wave and time-domain EPR imaging and Overhauser-enhanced magnetic resonance imaging of small animals: instrumental developments and comparison of relative merits for functional imaging, NMR Biomed. 17 (2004) 263–294.
- [11] S. Som, L. Potter, R. Ahmad, P. Kuppusamy, A parametric approach to spectralspatial EPR imaging, J. Magn. Reson. 186 (2007) 1–10.
- [12] R. Ahmad, D. Vikram, B. Clymer, L. Potter, Y. Deng, P. Srinivasan, J. Zweier, P. Kuppusamy, Uniform distribution of projection data for improved reconstruction quality of 4D EPR imaging, J. Magn. Reson. 187 (2007) 277–287.
- [13] Y. Deng, P. Kuppusamy, J. Zweier, Progressive EPR imaging with adaptive projection acquisition, J. Magn. Reson. 174 (2005) 177–187.
- [14] O. Grinberg, A. Smirnov, H. Swartz, High spatial resolution multi-site EPR oximetry: the use of a convolution-based fitting method, J. Magn. Reson. 152 (2001) 247–258.
- [15] S. Som, L. Potter, R. Ahmad, D. Vikram, P. Kuppusamy, EPR oximetry in three spatial dimensions using sparse spin distribution, J. Magn. Reson. 193 (2008) 210–217.
- [16] C. Poole Jr., Electron Spin Resonance: A Comprehensive Treatise on Experimental Techniques, Dover, Mineola, 1997.

- [17] M. Alecci, S. McCallum, D. Lurie, Design and optimization of an automatic frequency control system for a radiofrequency electron paramagnetic resonance spectrometer, J. Magn. Reson. 117 (1995) 272–277.
- [18] J. Hyde, W. Froncisz, A. Kusumi, Dispersion electron spin resonance with the loop-gap resonator, Rev. Sci. Instrum. 53 (1982) 1934–1937.
- [19] J. Hyde, H. Mchaourab, T. Camenisch, J. Ratke, R. Cox, W. Froncisz, EPR detection by time-locked sub-sampling, Rev. Sci. Instrum. 69 (1998) 2622– 2628.
- [20] J. Hyde, T. Camenisch, J. Ratke, R. Strangeway, W. Froncisz, Biomedical EPR, Part B: Methodology, Instrumentation, and Dynamics, Springer, New York, 2004.
- [21] S. Yen, Parametric estimation using electron paramagnetic resonance spectral models of over-modulated Lorentzian absorption and dispersion harmonics, Master's thesis, Department of Electrical and Computer Engineering, Ohio State University, 2008.
- [22] M. Tseitlin, O. Tseitlin, Using of digital demodulation of multiharmonic overmodulated EPR signals to improve EPR oximetry reliability, Appl. Magn. Reson. 36 (2009) 25–34.
- [23] M. Tseitlin, V. Iyudin, O. Tseitlin, Advantages of digital phase-sensitive detection for upgrading an obsolete CW EPR spectrometer, Appl. Magn. Reson. 35 (2009) 569–580.
- [24] B. Porat, A Course in Digital Signal Processing, Wiley, New York, 1996.
- [25] J. Hyde, J. Gajdzinski, EPR automatic frequency control circuit with field effect transistor (FET) microwave amplification, Rev. Sci. Instrum. 59 (1988) 1352– 1356.
- [26] B. Leugn, The oversampling technique for analog to digital conversion: a tutorial overview, Analog Integr. Circ. Sig. 1 (1991) 65–74.
- [27] R. Strangeway, T. Ishii, J. Hyde, Low-phase-noise Gunn diode oscillator design, IEEE Trans. Microwave Theory Tech. 36 (1988) 792–794.
- [28] G. Rinard, R. Quine, B. Ghim, S. Eaton, G. Eaton, Easily tunable crossed-loop (Bimodal) EPR resonator, J. Magn. Reson. 122 (1996) 50–57.
- [29] M. Tseitlin, R. Quine, G. Rinard, S. Eaton, G. Eaton, Combining absorption and dispersion signals to improve signal-to-noise for rapid-scan EPR imaging, J. Magn. Reson. 203 (2010) 305–310.
- [30] R. Quine, G. Eaton, Setting the microwave phase in an EPR spectrometer, J. Magn. Reson 119 (1995) 268–270.
- [31] Y. Deng, R. Pandian, R. Ahmad, P. Kuppusamy, J. Zweier, Application of magnetic field over-modulation for improved EPR linewidth measurements using probes with Lorentzian lineshape, J. Magn. Reson. 181 (2006) 254– 261.
- [32] R. Pandian, V. Dang, P. Manoharan, J. Zweier, P. Kuppusamy, Effect of nitrogen dioxide on the EPR property of lithium octa-n-butoxy 2,3-naphthalocyanine (LiNc-BuO) microcrystals, J. Magn. Reson. 181 (2006) 154–161.
- [33] G. Feher, Sensitivity considerations in microwave paramagnetic resonance absorption techniques, Bell Sys. Tech. J. 36 (1957) 449–484.
- [34] P. Vanassche, G. Gielen, W. Sansen, A generalized method for computing oscillator phase noise spectra, in: Proceedings of the International Conference on Computer-Aided Design, 2003, pp. 247–250.
- [35] V. Krymov, G. Gerfen, Analysis of the tuning and operation of reflection resonator EPR spectrometers, J. Magn. Reson. 162 (2003) 466–478.
- [36] D. Stephens, Phase-Locked Loops for Wireless Communications: Digital, Analog and Optical Implementations, Kluwer Academic, Norwell, 2002.